

Non-parametric Bayesian graph models reveal community structure in resting state fMRI

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Abstract

Modeling of resting state functional magnetic resonance imaging (rs-fMRI) data using network models is of increasing interest. It is often desirable to group nodes into clusters to interpret the communication patterns between nodes. In this study we consider three different nonparametric Bayesian models for node clustering in complex networks. In particular, we test their ability to predict unseen data and their ability to reproduce clustering across datasets. The three generative models considered are the Infinite Relational

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Model (IRM), Bayesian Community Detection (BCD), and the Infinite Diagonal Model (IDM). The models define probabilities of generating links within and between clusters and the difference between the models lie in the restrictions they impose upon the between-cluster link probabilities. IRM is the most flexible model with no restrictions on the probabilities of links between clusters. BCD restricts the between-cluster link probabilities to be strictly lower than within-cluster link probabilities to conform to the community structure typically seen in social networks. IDM only models a single between-cluster link probability, which can be interpreted as a background noise probability. These probabilistic models are compared against three other approaches for node clustering, namely Infomap, Louvain modularity, and hierarchical clustering. Using 3 different datasets comprising healthy volunteers' rs-fMRI we found that the BCD model was in general the most predictive and reproducible model. This suggests that rs-fMRI data exhibits community structure and furthermore points to the significance of modeling heterogeneous between-cluster link probabilities.

Keywords: complex network, graph theory, infinite relational model, Bayesian community detection, resting state fMRI

Highlights

1. Three nonparametric Bayesian models for node clustering are used to model rs-fMRI.
2. Models' predictability and reproducibility are extensively evaluated using resampling.
3. The community structure model shows better predictability and repro-

ducibility.

4. This finding suggests that rs-fMRI graphs exhibit community structure.
5. Modeling between-cluster link probabilities adds important information.

1 **1. Introduction**

2 Analysis of resting state functional magnetic resonance imaging (rs-fMRI)
3 has emerged as a powerful research tool to study whole-brain functional con-
4 nectivity. Since rs-fMRI provides information about intrinsic fluctuations in
5 functional connectivity within and among brain networks, many conventional
6 analysis schemes applied in task-related fMRI studies are irrelevant. Hence,
7 a number of new techniques have been developed based on identification of
8 stable spatio-temporal multivariate structure in the brain wide set of blood
9 oxygen level dependent (BOLD) time series.

10 Using correlation methods or flexible multivariate techniques like inde-
11 pendent component analysis (ICA) it has been shown that the BOLD sig-
12 nals of distant brain regions are coordinated suggesting interaction as they
13 form so-called resting-state networks. The number and precise definition of
14 these networks are controversial but several networks are broadly accepted,
15 including the default mode network, motor network, visual network, fronto-
16 parietal, dorsal attention network (Damoiseaux et al., 2006). In addition to
17 signals reflecting neuronal activity, the BOLD signal may be contaminated
18 by physiological noise stemming from respiratory and cardiac cycles and head
19 motion (Birn et al., 2006; Power et al., 2014).

20 Complex network analysis is a very active research field (Barabási, 2003)

21 that has already found application in neuroimaging and in modeling resting
22 state connectivity (Bullmore and Bassett, 2011; Sporns, 2011). The basic
23 object is the 'network graph'. When applied to neuroimage analysis the
24 network graph is formed by brain regions represented as nodes. Nodes are
25 connected by a link if brain regions are co-activated above a certain threshold.
26 In rs-fMRI co-activation is often measured simply by calculating correlation
27 between time series.

28 Network structure can be studied at many levels, from local motifs to
29 global features like scale free link distributions signifying long-range coordi-
30 nation (van den Heuvel et al., 2008). Likewise, dense connections between
31 high degree nodes is referred to as 'rich club organization' (van den Heuvel
32 and Sporns, 2011). At the intermediate level we may identify clusters of
33 highly linked nodes, i.e., high within-cluster link density and low link den-
34 sity to nodes in other clusters. By analogy to social networks such groups
35 are referred to as *communities*. The presence of community structure in a
36 network can be quantified by the global *modularity* index (Newman, 2006).
37 Modularity can also be used to identify communities, i.e., by clustering nodes
38 such that the modularity index is maximized (Newman, 2006; Lehmann and
39 Hansen, 2007). Bassett et al. (2011) showed that 'flexibility', a measure for
40 the number of cluster-assignment changes for nodes in a modularity opti-
41 mized node-partition across time, is predictive for the amount of learning in
42 a motor task in a subsequent session. Stevens et al. (2012) showed that mod-
43 ularity predicts visual working memory capacity, and Meunier et al. (2009)
44 found that modularity is reduced during normal aging. Likewise, evidence
45 is emerging that global modularity can be used as a bio-marker. For in-

46 stance patients with childhood-onset schizophrenia have reduced modularity
47 of their resting state networks (Alexander-Bloch et al., 2010). However, fo-
48 cusing on modularity as the single summary of a complex network may be
49 overly simplistic as the modularity measure does not account for variability
50 in the inter-linking relations between functional clusters. Hence, modularity
51 driven clustering might not reveal all salient aspects of community structure
52 in a network. Indeed, modularity has been criticized for its lack of flexibility
53 as a measure of community structure (Fortunato and Barthélemy, 2007).

54 A better understanding of this important mid-level structure in brain net-
55 works requires methods that can capture more informative representations
56 of community structure. For this we turn to a family of expressive generative
57 network models. Relational Models are statistical generalizations of graph
58 clustering that consider not only the within-cluster density but also take
59 the specific relations between clusters into consideration. The Infinite Rela-
60 tional Model (IRM) (Kemp et al., 2006; Xu et al., 2006) is a non-parametric
61 generalization of the stochastic block model (Nowicki and Snijders, 2001),
62 for inference of such generalized group structure in complex networks. As
63 the IRM representation considers both linking within and between groups,
64 a highly inter-linked group of nodes could in fact be clustered in different
65 groups if they link in different ways to other clusters, i.e., the IRM can infer
66 more general group structures beyond the conventional community structure.
67 An additional feature of the IRM type of model is that it conveniently allows
68 for analysis of multi-graph networks, which for neuroimaging data could be
69 graphs from multiple sessions or subjects. For multi subject analysis one
70 could look for a common node clustering structure over subjects but allow

71 individual subject cluster linking densities (Mørup et al., 2010) or test the
72 hypothesis that both clustering and link structure are shared between all
73 subjects (Andersen et al., 2012b).

74 A constrained variant of the IRM representing the community structure
75 of graphs in the sense of grouping highly connected node sets was proposed
76 recently by Mørup and Schmidt (2012). The Bayesian Community Detection
77 (BCD) scheme restricts the between-cluster link densities to be strictly lower
78 than within-cluster link densities, thus constraining the more general IRM to
79 conform with the notion of a community in a social network. Another con-
80 straint is introduced by the so-called Infinite Diagonal Model (IDM) (Mørup
81 and Schmidt, 2012; Schmidt and Mørup, 2013). The IDM allows for differ-
82 ential within-cluster link densities but models only a single between-cluster
83 density and as such the variability in the link densities between clusters is
84 neglected when inferring the clustering structure. Since the between-cluster
85 link density is shared across clusters, it can be thought of as a background-
86 noise density.

87 It should be noted that certain metrical properties can be expected when
88 basing the graph on simple time series correlation, thereby assuming station-
89 arity. If a node A is highly correlated with node B , and B is highly correlated
90 with C , then there is a lower limit on the correlation between nodes A and
91 C which can be inferred by the triangle inequality (Zalesky et al., 2012).
92 This bound will support the formation of community structure, as in so-
93 cial relations: 'Friends of friends are friends', however, we also note that by
94 thresholding the correlation, the impact on the community structure of these
95 geometrical constraints is non-trivial.

96 Spatial grouping of brain regions by similarity of BOLD time series as
 97 pursued in the present work can be seen as complementary to classical ap-
 98 proaches to spatial grouping such as time series clustering (Goutte et al.,
 99 1999) and independent component analysis (ICA) (McKeown et al., 1998,
 100 2003). Compared with conventional clustering, the relational modeling ap-
 101 proach has the advantage that clusters are formed by considering the connec-
 102 tivity patterns both within and between clusters, and furthermore relational
 103 models avoid the formation of a group prototype, hence allow for more flexible
 104 group structures to be found (Kemp et al., 2006). The use of ICA is based
 105 on assumptions of independence either in spatial or temporal dimensions,
 106 which can be questioned in the resting state as it has been observed that
 107 components are negatively correlated in time and have extensive overlaps in
 108 space (Fox et al., 2005).

109 In this study, we apply the above-mentioned community detection sche-
 110 mes to rs-fMRI data acquired in three cohorts of healthy volunteers and in-
 111 vestigate to which degree functional brain networks as measured by rs-fMRI
 112 exhibit community structure. The three Bayesian relational methods, i.e.
 113 IRM, BCD, and IDM, for inference of group structure in complex networks
 114 differ only in the way the link probabilities between clusters are modeled. The
 115 rich link structures of the relational models can be seen as a way of inferring
 116 functional integration at the inter-community level as discussed in (Hagmann
 117 et al., 2008; Sporns, 2013). We evaluate the performance of these models with
 118 respect to their ability to predict out-of-sample data (predictability) and the
 119 robustness of their clustering under re-sampling of data (reproducibility) us-
 120 ing the NPAIRS split-half framework (Strother et al., 2002). The evaluation

121 is carried out on three datasets from different sites and the models are eval-
122 uated both within and between sites for several thresholds of the correlation
123 matrices. In addition, we compare the three models with three other meth-
124 ods for grouping nodes into clusters, namely Infomap, Louvain modularity,
125 and hierarchical clustering. The work in this paper builds on work presented
126 in (Andersen et al., 2012b).

127 **2. Methods**

128 For generality we investigate three rs-fMRI datasets. One dataset ac-
129 quired locally at the Danish Research Centre for Magnetic Resonance (Copen-
130 hagen) and two other rs-fMRI datasets publicly available in the FCON1000
131 database (Biswal et al., 2010) (viz., the 'Beijing' and the 'Leipzig' datasets).

132 *2.1. Copenhagen data*

133 The Copenhagen dataset included 30 healthy controls with no history
134 of neurological or psychiatric disease. At the day of scanning all subjects
135 were asked to refrain from caffeine, cigarettes or alcohol intake at least six
136 hours prior to the scanning session. All subjects gave written informed con-
137 sent prior to scanning and the study was approved by the local scientific
138 ethics committee of Copenhagen and Frederiksberg Communities (protocol
139 no. KF01 - 131/03 with addendum). The Edinburgh handedness inventory
140 (Oldfield, 1971) revealed that all participants except two were right handed.

141 All MRI measurements were performed on a 3.0 Tesla Magnetom Trio
142 scanner (Siemens, Erlangen, Germany). Each participant underwent an MRI
143 session including a structural scan as well as a functional scan during rest
144 both with full brain coverage. During the functional scan subjects were

145 instructed to rest with their eyes closed without falling asleep, and refrain
146 from any voluntary motor or cognitive activity.

147 The first scan during each session was the rs-fMRI functional scan which
148 consisted of a T2* weighted echo planar imaging (EPI) sequence with a
149 repetition time of 2490 ms, echo time 30 ms and flip angle 90 degrees. Over
150 a period of 20 minutes we collected 480 brain volumes each consisting of 42
151 axial slices with an isotropic resolution of 3 mm, field of view (FOV): 192x192
152 mm. During scanning we monitored the subjects cardiac and respiratory
153 cycles using an infrared pulse oximeter and a pneumatic thoracic belt. The
154 structural scan was based on a magnetization prepared rapid gradient echo
155 (MPRAGE) sequence with the following parameters: Repetition time (TR)
156 = 1550 ms, echo time (TE) = 3.04 ms, inversion time (IT) = 800 ms; 192
157 sagittal slices; 1 mm isotropic resolution; FOV = 256 mm; flip-angle = 9
158 degrees.

159 The functional images were preprocessed using statistical parametric map-
160 ping software (SPM8, Wellcome Trust Centre for Neuroimaging, [http://](http://www.fil.ion.ucl.ac.uk/spm)
161 www.fil.ion.ucl.ac.uk/spm) implemented in Matlab 7.9 (MathWorks, Mas-
162 sachusetts, USA). In order to allow stabilization of T1 equilibrium effects we
163 discarded the first five volumes prior to analysis. The remaining 475 brain
164 volumes were realigned to the time-series mean using a two-step procedure
165 and then co-registered to the same-session T1-weighted MPRAGE scan by
166 a 6-parameter rigid-body transformation. The T1-weighted scan was spa-
167 tially normalized to the Montreal Neurological Institute (MNI) 305 standard
168 template using the unified segmentation/normalisation procedure as imple-
169 mented in SPM8 (Ashburner and Friston, 2005). Subsequently the same

170 normalisation parameters were used to normalise the EPI images.

171 Both hardware instability and unwanted physiological effects (such as car-
172 diac pulsation and respiration) produce signal changes in fMRI time-series
173 (Smith et al., 1999; Dagli et al., 1999; Glover et al., 2000; Lund et al., 2006).
174 These signal changes may give rise to signal fluctuation resembling those typ-
175 ically observed in rs-fMRI data (Birn et al., 2006). In order to reduce these
176 effects prior to extraction of time series for the regions of interest we applied
177 comprehensive temporal filtering of cardiac, respiratory and motion related
178 effects. The filter included a high-pass filter based on discrete cosine basis
179 functions (cut-off frequency 1/128 Hz). Cardiac and respiratory cycles were
180 modeled using Fourier expansions of the aliased cardiac (10 parameters) and
181 respiratory (6 parameters) cycles as well as first order cardiac by respiration
182 cycles interaction (4 parameters) effects (Glover et al., 2000). Residual mo-
183 tion effects (24 parameters) were modeled using a Taylor expansion of the
184 estimated movement parameters including spin-history effects (Friston et al.,
185 1996). Changes in the respiration volume over time has been demonstrated
186 to produce signal changes resembling those observed in rs-fMRI (Birn et al.,
187 2006). We model these changes by included 41 time delayed versions (time
188 delay between 20 and -20 seconds in one second intervals) of the respiration
189 volume. Finally the filter included individual time series from cerebrospinal
190 fluid voxels and white matter voxels from both the right and left hemispheres.
191 In total the linear filter included 108 regressors leaving 367 degrees of freedom
192 for the data.

193 2.2. *Beijing and Leipzig data*

194 Two other datasets were used from the FCON1000 database (Biswal et al.,
 195 2010) (http://fcon_1000.projects.nitrc.org). See Appendix A for a
 196 list of subjects used. The Beijing dataset consists of 42 of the subjects
 197 from the Beijing Zang set. The dataset is recorded with 33 slices using
 198 TR=2000ms and with 225 brain volumes. The Leipzig dataset consists of 37
 199 subjects (21 females), ages 20-42, TR=2300ms, 34 axial slices, and 195 brain
 200 volumes. For both datasets the first 5 volumes had already been discarded.
 201 Preprocessing was done in SPM8 and included realigning to time-series mean
 202 for motion correction and normalising to standard MNI space using the tem-
 203 plate EPI image included in SPM.

204 2.3. *Graph construction*

205 We extracted the mean signal in each of the 116 regions covered in the
 206 AAL database (Tzourio-Mazoyer et al., 2002) and constructed the correla-
 207 tion matrix for each subject. Since this matrix is symmetric only the upper
 208 diagonal is further considered. Each subject’s correlation matrix was bina-
 209 rized at an individual level to maintain the highest d -percent correlations
 210 corresponding to having a graph link density at d -percent. After threshold-
 211 ing an adjacency matrix \mathbf{A} is retrieved where $A_{i,j}$ is the (i, j) -th element of
 212 \mathbf{A} and $A_{i,j} = 1$ if there is a link between nodes i and j and $A_{i,j} = 0$ other-
 213 wise. Since we model multiple subjects, $\mathbf{A}^{(n)}$ denotes the adjacency matrix
 214 corresponding to subject n .

215 2.4. The models

216 This section will provide an overview of the models considered in this
217 paper. For a more in depth description please refer to (Schmidt and Mørup,
218 2013). The goal is to group nodes into non-overlapping clusters, such that
219 a common node-clustering across subjects is retrieved. Let \mathbf{z} be the vector
220 of nodes assignments where z_i takes the integer value corresponding to the
221 cluster index node i belongs to. The models used are all generative models
222 meaning that given the model definition and the model parameters one can
223 generate new graphs by drawing samples from the model. The models differ
224 in the way they model the link probability between and within clusters. Let
225 $\rho_{k,l}$ represent the link probability between clusters k and l . Since we here
226 consider undirected graphs ρ is symmetric.

227 2.4.1. The Infinite Relational Model

228 In IRM link probabilities within and between clusters are modeled in-
229 dividually and without restrictions. As such the model allows for complex
230 relations between clusters, and thus allows for flexible clustering of nodes.

231 Consider generating graphs from this model. The first step is to draw as-
232 signments of nodes into clusters, which is done using the Chinese Restaurant
233 Process (CRP) (Aldous, 1985) using the hyper-parameter α . The CRP gener-
234 ates a cluster assignment, where α controls the number of clusters generated,
235 where larger α will generate more clusters. Next, the link probabilities within
236 and between clusters $\rho_{k,l}$ are generated from the symmetric Beta distribu-
237 tion using the hyper-parameter β . Finally, the cluster assignments and the
238 link densities are used to generate links between nodes. This is done using
239 the Bernoulli distribution, where the probability of a link (success) between

240 nodes i and j is determined by the clusters (z_i and z_j) the nodes belong to.

241 The generative model can be summarized as:

| Infinite Relational Model | |
|---------------------------|--|
| Cluster assignments: | $\mathbf{z} \sim \text{CRP}(\alpha)$ |
| Link probabilities: | $\rho_{k,l} \sim \text{Beta}(\beta, \beta)$ |
| Links: | $A_{i,j}^{(n)} \sim \text{Bernoulli}(\rho_{z_i, z_j})$ |

242 In Appendix B.1 we derive the likelihood function for the IRM which is used
243 in model inference.

244 2.4.2. Infinite Diagonal Model

245 The model termed Infinite Diagonal Model (IDM) (Mørup and Schmidt,
246 2012) is a special case of the IRM where link probabilities between clusters
247 are constrained to be equal. As such, the IDM does not model the relation
248 between clusters but has a constant background link probability. The only
249 difference in terms of the model formulation is then

$$250 \quad \rho_{k,l} = \begin{cases} \rho_{k,k} & \text{if } k = l \\ \rho_b & \text{otherwise.} \end{cases}$$

251 2.4.3. Bayesian Community Detection

252 A network community is defined as a group of nodes with more dense link-
253 ing internally than externally. The Bayesian Community Detection (BCD)
254 model proposed in (Mørup and Schmidt, 2012) enforces larger within-cluster
255 link probabilities than between-cluster link probabilities. Like IRM, the clus-
256 ter assignments are first generated using the CRP. A cluster-gap is then

257 drawn from a symmetric Beta distribution with hyperparameter v . The
 258 within-cluster link probabilities are then drawn for each cluster again us-
 259 ing the Beta distribution. The between-cluster link probabilities are subse-
 260 quently drawn using the incomplete Beta distribution $\text{BetaInc}(a, b, x)$ con-
 261 strained to the interval $[0, x]$, with the density, $p(\theta) = \frac{1}{B_x(a, b)} \theta^{a-1} (1 - \theta)^{b-1}$,
 262 where $B_x(a, b)$ is the incomplete beta function. Thus, a draw from the in-
 263 complete Beta distribution will return a value between $[0, x]$, which can then
 264 be used to control the maximal value the between-cluster link probability can
 265 take. By setting x to the cluster-gap times the within-cluster link probability,
 266 the between-cluster link probability between two clusters k and l can then
 267 at most be as high as the smaller of the two within-cluster link probabilities
 268 multiplied by the cluster gap. The lower the gap-value the higher difference
 269 in within and between-cluster link probability. Finally, links are drawn using
 270 the Bernoulli distribution just like the other models. The generative model
 271 for BCD can thus be summarized as:

Bayesian Community Detection

Cluster assignments : $\mathbf{z} \sim \text{CRP}(\alpha)$

Cluster gap : $\gamma \sim \text{Beta}(v, v)$

Link probability : $\rho_{k,l} \sim \begin{cases} \text{Beta}(\beta, \beta) & \text{if } k = l \\ \text{BetaInc}(\beta, \beta, w_{k,l}) & \text{otherwise.} \end{cases}$

where $w_{k,l} = \min[\gamma\rho_{ll}, \gamma\rho_{kk}]$

Links : $A_{i,j}^{(n)} \sim \text{Bernoulli}(\rho_{z_i, z_j})$

272 2.5. Example 1

273 For illustration we generate a graph consisting of 50 nodes from each of
 274 the three models with $\alpha = 5, \beta = 1$. For the BCD model we set $v = 1$.
 275 Figure 1 shows the generated graphs. The plots are a combination of both
 276 the cluster assignment matrix, the adjacency matrix, and the link probability
 277 matrix. The adjacency matrix \mathbf{A} is plotted, where links between nodes are
 278 indicated by small black dots. Cluster membership is indicated with the
 279 colors to the left and top of the adjacency matrix and the link probability
 280 matrix is indicated with gray shaded background. For IRM there are no
 281 restrictions in the link probability values, resulting in some between-cluster
 282 link probabilities being larger than within-cluster link probabilities. For the
 283 BCD model the between-cluster link probability between two clusters are
 284 restricted to be smaller than the within-cluster link probability times the
 285 gap. The gap was drawn from the Beta distribution and in this case the gap
 286 is $\gamma = 0.96$. For the IDM model all the between-cluster link probabilities are
 287 equal meaning that clusters are only defined in the way they link internally
 288 in the clusters.

289 2.6. IRM and IDM model inference

290 In the previous sections we defined the generative models, which allow
 291 one to generate data by sampling from the model. However, we are inter-
 292 ested in inferring the model parameters given the data. By using the model
 293 definition the joint likelihood can be written and by using Bayes theorem
 294 an expression for the posterior distribution can be found. It is then possible
 295 to sample from this posterior distribution using Markov chain Monte Carlo
 296 sampling (MCMC) methods. For IRM and IDM the link probabilities can

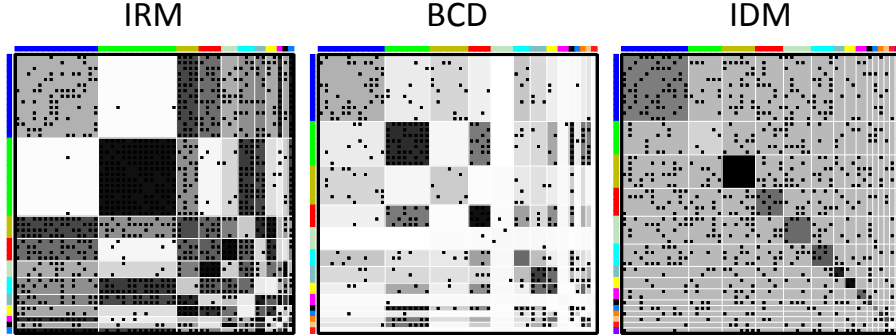


Figure 1: Example 1. Figure illustrating data drawn from each of the three models, IRM, BCD, and IDM respectively. Plots illustrates both the adjacency matrix \mathbf{A} (links indicated by small black squared dots), cluster membership \mathbf{z} as color codes to the left and top of the adjacency matrix, and link probability matrix ρ as gray shading of the matrix elements.

analytically be integrated out which means that we only have to sample over the node assignments. For that Gibbs sampling in combination with split-merge Metropolis-Hastings updates (Jain and Neal, 2004; Kemp et al., 2006; Mørup et al., 2010) is used. Below is a description of these two steps.

Gibbs sampling is a Markov-chain Monte Carlo sampling method. For each scan of the Gibbs sampler each node’s cluster assignment is updated using the conditional distribution of that node’s assignment given the assignments of the remaining nodes. For IRM the conditional distribution is derived in Appendix B.1 (equation B.2) and for IDM it is derived in Appendix B.2 (equation B.3).

Given the incremental nature of the Gibbs sampling algorithm it has difficulties escaping local maxima of the probability landscape. For instance it is hard to split a single cluster into two new clusters since this requires that nodes are moved one at a time from a cluster to the other cluster. To

311 overcome this we use a restricted split-merge sampling scheme (Jain and
 312 Neal, 2004), which potentially merges two existing clusters into one or split
 313 a single cluster into two clusters. At each step of the algorithm two nodes
 314 are selected at random with uniform probability. If the two selected nodes
 315 currently are assigned different clusters then an assignment is proposed where
 316 these two clusters are merged into one cluster. On the contrary, if these
 317 two selected nodes are currently assigned to the same cluster then a new
 318 assignment is proposed where all nodes assigned to this cluster are split into
 319 two separate clusters. The split-proposal is found using a restricted Gibbs-
 320 sampling procedure. First a launch state is found by allocating the two
 321 nodes to two different empty clusters as proposed in (Dahl, 2005). Then
 322 remaining nodes are in random order assigned to either of the two clusters
 323 based upon their conditional probability. This state is then referred to as the
 324 launch state. The launch state is refined by restricted Gibbs sampling steps
 325 where nodes from the two new clusters can be re-assigned either of the two
 326 clusters based on the conditional probability (equation B.2 and B.3). This
 327 procedure is restricted because only nodes from the cluster from which the
 328 nodes originally came from are re-assigned and they can only be assigned to
 329 either of the two new clusters. The proposed configuration is then sampled
 330 from the launch state. If this proposed state \mathbf{z}^* in the Markov chain is
 331 accepted with the Metropolis-Hasting acceptance probability $a(\mathbf{z}^*, \mathbf{z})$ then
 332 this becomes the new state else the old state \mathbf{z} is kept as the new state.
 333 The acceptance probability is given as $a(\mathbf{z}^*, \mathbf{z}) = \min \left[1, \frac{q(\mathbf{z}|\mathbf{z}^*)}{q(\mathbf{z}^*|\mathbf{z})} \frac{\pi(\mathbf{z}^*)}{\pi(\mathbf{z})} \right]$, where
 334 $\pi(\mathbf{z}) = P(\mathbf{A}|\mathbf{z})P(\mathbf{z})$ (please see Appendix B) and $q(\mathbf{z}^*|\mathbf{z})$ is the probability
 335 of transition from \mathbf{z} to \mathbf{z}^* . For further detail about the split-merge sampling

336 please refer to Jain and Neal (2004).

337 2.7. BCD model inference

338 In IRM and IDM we are able to marginalize link probabilities ($\boldsymbol{\rho}$) out.
339 This is not the case in BCD because between-cluster link probabilities are
340 dependent of the within-cluster link probabilities. However, the vast ma-
341 jority of the parameters, namely the between-cluster link probabilities, can
342 be integrated out (Appendix B.3). The remaining parameters \mathbf{z} , $\dot{\boldsymbol{\rho}}$, and γ
343 are sampled using MCMC, where $\dot{\boldsymbol{\rho}}$ refer to the within-cluster link proba-
344 bilities (the diagonal of $\boldsymbol{\rho}$). The within-cluster link probabilities and cluster
345 gaps are sampled with Metropolis-Hastings. The cluster assignments \mathbf{z} are
346 like the IRM sampled with Gibbs sampling and split-merge moves, however
347 new possible values for the within link probabilities and cluster gaps are first
348 drawn from their prior. In Appendix B.3 we derive the conditional distribu-
349 tions used in the sampling. For further information please see (Mørup and
350 Schmidt, 2012).

351 2.8. Example 2

352 We illustrate differences in cluster assignments and link probabilities in-
353 ferred by each of the three models. We generate a synthetic graph with
354 40 nodes, 10 nodes in each of four clusters. The example is designed such
355 that *cluster1* and *cluster2* share the same within and between-cluster link
356 probabilities, however only *cluster2* is connected with *cluster3*. *Cluster3* and
357 *cluster4* have low within-cluster probabilities but high between-cluster link
358 probability. *Cluster3* and *cluster4* are not connected to *cluster1* and *clus-*
359 *ter2*. The first row in Figure 2 show the true assignment vector (\mathbf{z}) coded as

360 a 1-of-n matrix and the true link probabilities. The next rows show the as-
 361 signments and link probabilities inferred by the IRM, BCD, and IDM models
 362 respectively. Except for a single node IRM finds the correct grouping struc-
 363 ture. BCD assigns the first two clusters correctly and mislabels the same
 364 node as IRM, but BCD has difficulties with the remaining nodes because the
 365 true model has higher between-cluster than within-cluster link probabilities.
 366 Since IDM does not model the between-cluster link probabilities, it groups
 367 the first two clusters together and the next two clusters together.

368 *2.9. NPAIRS Evaluation Criteria*

369 To evaluate the performance of the models, we used the NPAIRS split-
 370 half evaluation framework (Strother et al., 2002). Under this framework
 371 the set of subjects were split into two half-splits (S1 and S2) and models
 372 were inferred on each half-split enabling us to estimate the predictability
 373 and reproducibility of the models. The models' predictability was evaluated
 374 using test log likelihood. The node assignment and link probabilities from
 375 the sample with the highest value of the posterior distribution were used to
 376 calculate the test log likelihood of the other split. The test log likelihood
 377 was calculated for both splits (with the other split as training data) and
 378 the average test log likelihood was calculated and used as the predictability
 379 measure. The test log likelihood for split S2 (using the model parameters
 380 inferred using split S1) was calculated by

$$\begin{aligned}
 381 \quad & \log P(\mathbf{A}^{\text{S2,(1)}}, \dots, \mathbf{A}^{\text{S2,(N)}} | \boldsymbol{\rho}, \mathbf{z}) = \\
 382 \quad & \frac{1}{N} \sum_{n=1}^N \sum_{j>i} \left[A_{i,j}^{\text{S2,(n)}} \log(\rho_{z_i, z_j}) + (1 - A_{i,j}^{\text{S2,(n)}}) \log(1 - \rho_{z_i, z_j}) \right]. \quad (1)
 \end{aligned}$$

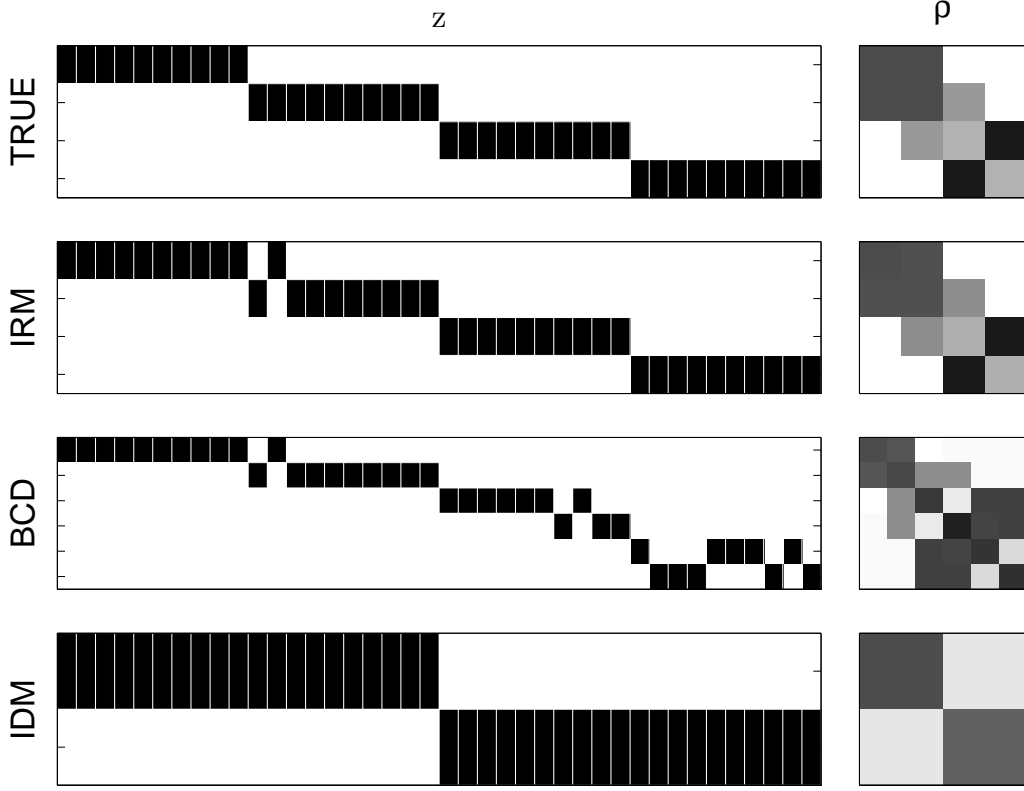


Figure 2: Example 2. First row show the true assignments coded as a 1-of-n matrix and the true link probabilities. The next rows show the structure and link probabilities inferred by IRM, BCD, and IDM respectively.

383 We measured the reproducibility of the models using normalized mutual in-
 384 formation between assignment matrices (\mathbf{z}^{S1} and \mathbf{z}^{S2}) of the sample with the
 385 highest value of the posterior distribution inferred using the two different
 386 splits.

$$387 \quad \text{NMI} = \frac{2\text{MI}(\mathbf{z}^{S1}, \mathbf{z}^{S2})}{\text{MI}(\mathbf{z}^{S1}, \mathbf{z}^{S1}) + \text{MI}(\mathbf{z}^{S2}, \mathbf{z}^{S2})}, \quad (2)$$

388 where

$$389 \quad \text{MI}(\mathbf{z}^{\text{S1}}, \mathbf{z}^{\text{S2}}) = \sum_{k=1}^{D1} \sum_{l=1}^{D2} p(z^{\text{S1}} = k, z^{\text{S2}} = l) \log \left(\frac{p(z^{\text{S1}} = k, z^{\text{S2}} = l)}{p(z^{\text{S1}} = k)p(z^{\text{S2}} = l)} \right), \quad (3)$$

390 where $D1$ and $D2$ are the number of clusters inferred using S1 and S2, re-
391 spectively.

392 The model used in e.g. Mørup et al. (2010) used individual subject link
393 probabilities, that is, each subject was modeled with her own link proba-
394 bility matrix while sharing the node assignments \mathbf{z} . This allows for subject
395 variability in the communication between clusters and can be used to test
396 for differences in subject populations. However, here we are interested in the
397 models’ predictive abilities, that is, how well can a model and its param-
398 eters learned from a sub-group of subjects predict the graphs from another
399 group of subjects. Therefore we do not model individual subject link den-
400 sities but constrain $\boldsymbol{\rho}$ to be common across subjects. The derivation of the
401 models (Appendix B.1) reveals that this amounts to simply summing the
402 adjacency matrices across subjects $\sum_n \mathbf{A}^{(n)} = \mathbf{A}^{\text{tot}}$. This means that under
403 this restricted model definition inference of the latent variables of the model
404 does not scale with the number of graphs (subjects) and therefore our model
405 formulation allows for analysis of large numbers of subjects.

406 2.10. Experiments

407 The initial assignment of nodes to clusters might affect the final cluster-
408 ing, so we did some initial experiments with different number (1, 20, 50, or
409 116) of initial clusters (data not shown). For IRM and BCD, the similarity
410 between different choices were in general very high (mean NMI > 0.95) with
411 a tendency of generating more clusters when initializing all nodes in its own

412 cluster. For the IDM the initialization had a greater impact on the final
 413 clustering. Initialization in few (1 or 20) clusters showed greater variability
 414 in the final clustering whereas initialization in 50 or 116 clusters showed
 415 more stable final clustering. Thus to compromise, in all the experiments described
 416 below, nodes were randomly assigned to one of 50 clusters and the
 417 sampler ran for 500 iterations. The sample with the highest value of the
 418 posterior distribution was then used as representative for a given run. In all
 419 experiments $\alpha = \beta = 1$.

420 2.10.1. *Estimated clusters*

421 To inspect the clustering of the different models, the inference procedure
 422 was launched 10 times for each model using the graph link density $d = 8\%$
 423 and the sample with the overall highest value of the posterior distribution
 424 across the 10 runs was visualized. The reproducibility measured as the mean
 425 NMI between the samples with the highest value of the posterior distribution
 426 for each run was calculated. As the inference is stochastic, this measures the
 427 methods' ability to reproduce clusterings for different restarts. Likewise, the
 428 clustering similarity between the methods was also estimated by calculating
 429 the mean NMI between each pair of the 10 solutions found.

430 In addition, we investigated the impact on different choices of graph link
 431 density. For each of the densities $d = 2\%, 4\%, 8\%, 16\%, 32\%$ we launched
 432 the inference 10 times for each model and estimated the mean NMI between
 433 densities within each model. The clustering with the highest value of the
 434 posterior distribution for each density was visualized for the BCD model.
 435 These experiments used all the subjects from the Copenhagen dataset.

436 *2.10.2. Predictability and reproducibility*

437 We asked how well the clusterings reproduce between datasets and how
438 well the models predict new data. To this end, we evaluated the models us-
439 ing the NPAIRS framework. Subjects were randomly split into two equally
440 sized groups and model inference was conducted on each split. The highest
441 posterior distribution sample was identified for the two splits and NMI be-
442 tween clusterings was calculated as a measure of the models' reproducibility.
443 Using the estimated link probability matrix and assignment from the sam-
444 ple with the highest value of the posterior distribution of one split, the test
445 log likelihood for the other split was calculated as a measure of the models'
446 predictability. This was done for 100 different half-splits of the Copenhagen
447 dataset using 8% graph link density.

448 *2.10.3. Predictability and reproducibility for various link densities*

449 For further evaluation of the methods the analysis were repeated within
450 each of the three datasets as well as between the datasets for graph link
451 densities of $d = 2\%, 4\%, 8\%, 16\%, 32\%$. For analysis done within each in-
452 dividual dataset the subjects were randomly split in half. For the between
453 dataset analysis, inference was done within each dataset and NMI and test
454 log likelihood was calculated between datasets. For each link density the log
455 likelihood ratio was calculated as the log likelihood of a random Erdős-Rényi
456 model having the considered link density divided by the log likelihood of
457 the inferred model. This makes the predictability measure more comparable
458 between link densities, however, we note that the log likelihood cannot di-
459 rectly be compared for different link densities as the data itself changes when
460 changing the link densities.

461 We compare the Bayesian methods with two of the best community detec-
 462 tion algorithms (Fortunato, 2010) as well as with a simple method based on
 463 hierarchical clustering. The first method is Infomap (Rosvall and Bergstrom,
 464 2008) using the C++ implementation available from [http://www.mapequation.](http://www.mapequation.org/)
 465 [org/](http://www.mapequation.org/). Infomap has previously been used for fMRI networks, see e.g. (Power
 466 et al., 2011). The second method is the so-called Louvain method (Blondel
 467 et al., 2008) as implemented in the Brain Connectivity Toolbox ([https:](https://sites.google.com/site/bctnet/)
 468 [//sites.google.com/site/bctnet/](https://sites.google.com/site/bctnet/)) (Rubinov and Sporns, 2010). This
 469 method is based on modularity optimization. The third method is the ag-
 470 glomerative hierarchical clustering based on average linkage using the Matlab
 471 function 'linkage'. For this method we formed clusters by thresholding the
 472 hierarchical tree at the distance 0.9.

473 To obtain a single clustering across a group of subjects we ran the meth-
 474 ods on the summed adjacency matrix across the subjects in each half-split.
 475 This summed adjacency matrix is also used for inference in the probabilistic
 476 models (as noted in section 2.9), which therefore allows for a comparison
 477 between methods. To compare the results from these three methods we treat
 478 the clustering found as it was produced by the IRM and thus calculate the
 479 link probabilities between clusters as it was done for the IRM model. This al-
 480 lows us to calculate the predictability for unseen data as described in Section
 481 2.9. In addition to the predictability and reproducibility we also evaluate
 482 the modularity index for all methods. The modularity index is given as
 483 $Q = \text{Tr}(\mathbf{Z}\mathbf{B}\mathbf{Z}^\top)/2m$ where \mathbf{Z} is 1-of-D encoding matrix of the link assign-
 484 ment vector \mathbf{z} and m is the number of links in the graph. $\mathbf{B} = \mathbf{A} - (\mathbf{k}\mathbf{k}^\top)/2m$
 485 is the modularity matrix where \mathbf{k} is the vector of node degrees.

486 3. Results

487 3.1. Estimated clusters

488 We thresholded the graphs to maintain the top 8% correlations. The
489 threshold correspond to a mean (std) p-value across subjects of $4.75 \cdot 10^{-5}$ ($1.80 \cdot$
490 10^{-4}). The reproducibility between solutions found with different restarts
491 was measured as the NMI between the sample with the highest value of the
492 posterior distribution for each run. This was done within all three methods
493 and between the methods and results are shown in table 1 along with the
494 number of clusters estimated by each of the methods. For all three meth-
495 ods the clustering for different initializations showed a very high consistency
496 as the NMI was greater than 0.96 for all methods. Also, the number of
497 estimated clusters was very consistent within method, but showed a great
498 between method variability where IRM estimated on average 35.7 clusters,
499 BCD estimated 41.0 and IDM estimated only 18.8. For BCD the mean (std)
500 gap parameter was estimated to 0.88 (0.02). The IRM and BCD clusterings
501 were found to be very similar with a mean NMI of 0.94. The IDM clustering,
502 however, was less similar to the other two methods with a mean NMI of 0.76
503 and 0.75 to IRM and BCD respectively.

504 In figure 3 the samples with the highest value of the posterior distribution
505 across the 10 runs for each method are visualized. The first column shows
506 the link probability matrix $\boldsymbol{\rho}$ which has been permuted such that clusters
507 with the greatest overlap between methods are first. The labels for the clus-
508 ters can be found in Appendix C. The matrix elements are color-coded in
509 grey-scale according to the value of the link probabilities and the size of the
510 matrix elements indicate the size of the clusters. The first 5 clusters were

| Method | IRM | BCD | IDM | Mean (std) D |
|--------|-------------|-------------|-------------|--------------|
| IRM | 0.96 (0.01) | - | - | 35.7 (1.25) |
| BCD | 0.94 (0.01) | 0.96 (0.02) | - | 41.0 (2.05) |
| IDM | 0.76 (0.02) | 0.75 (0.01) | 0.97 (0.02) | 18.8 (1.14) |

Table 1: The mean(std) of normalized mutual information (NMI) between the clustering of 10 runs within and between method along with the number of clusters (D) estimated with each of the three methods IRM, BCD, and IDM.

511 identical between the three methods. The next 12 clusters were identical
 512 between IRM and BCD while IDM had all these clusters in one large cluster.
 513 When looking at the link probabilities between these 12 clusters it is evident
 514 that there is a high link probability within and between these nodes, but sub-
 515 tle differences exist between the different clusters which caused the IRM and
 516 BCD to cluster them into separate clusters. Since IDM does not consider the
 517 between-cluster link probabilities these clusters were grouped together in the
 518 IDM method. The same was true for the next 6 clusters which were identical
 519 for the IRM and BCD and all lumped together in the IDM model since the
 520 link probabilities between these clusters were relatively high. The next three
 521 columns show the found clusters in posterior, lateral and superior views of
 522 the brain. The clusters are colored according to the colors shown next to
 523 the link probability matrices (and the labels given in Appendix C). Brain
 524 regions within clusters are connected with lines where line thickness indicates
 525 the average link density over subjects for the specific connection. This figure
 526 shows that the IRM and BCD clusterings were very similar. In general, these
 527 two methods produced clusters with relatively few nodes and grouped inter-
 528 hemispheric homologues areas together. IDM also grouped interhemispheric

529 homologues areas together, however, as just described this method does not
530 consider specific relations to other brain areas, which resulted in larger and
531 rather unspecific clusters. For instance the cluster colored in turquoise is a
532 cluster made up of 34 nodes including nodes in frontal, occipital, parietal,
533 and temporal lobes.

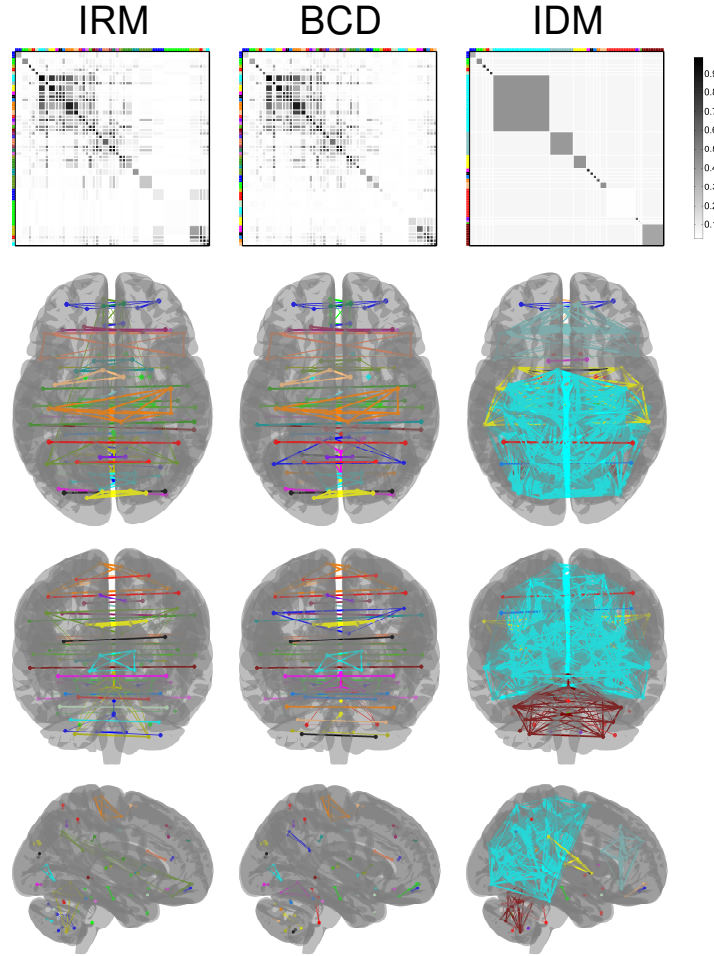


Figure 3: The extracted clusters using the three methods IRM, BCD, and IDM respectively. The first row shows the link probability matrices ρ , which have been permuted such that the order of the clusters corresponds across methods. The matrix elements are color-coded according to the value of the link probabilities and the size of the matrix element indicates the size of the respective cluster. The colors next to the matrices correspond to different clusters. The next three rows show the clusters in three different views (superior, posterior, and lateral) of the brain. The clusters are color coded according to the colors next to the link probability matrices and node assignment for each node can be found in Appendix C with the same color as plotted here. Different brain regions within each cluster are connected with lines where the thickness of the line indicates the average link density across subjects for the specific connection.

534 In figure 4 we show an example cluster and its connectivity to other
535 clusters. A cluster composed of left and right supplementary motor area
536 and left precentral gyrus (A) was selected. This cluster was identical for
537 IRM and BCD while results are not shown for IDM. The figure also displays
538 the 4 clusters with highest between-cluster link probabilities to this cluster.
539 These 4 clusters with highest link probabilities were: (B, $\rho_{A,B} = 0.732$)
540 left and right postcentral gyrus, left and right paracentral lobule and right
541 precentral gyrus; (C, $\rho_{A,C} = 0.714$) left and right middle cingulate gyrus;
542 (D, $\rho_{A,D} = 0.516$) left and right superior frontal gyrus; (E, $\rho_{A,E} = 0.456$)
543 left and right superior temporal gyrus. The line widths between clusters in
544 the figure reflect between-cluster link probabilities, likewise the widths of the
545 boxes reflect the within-cluster link probabilities.

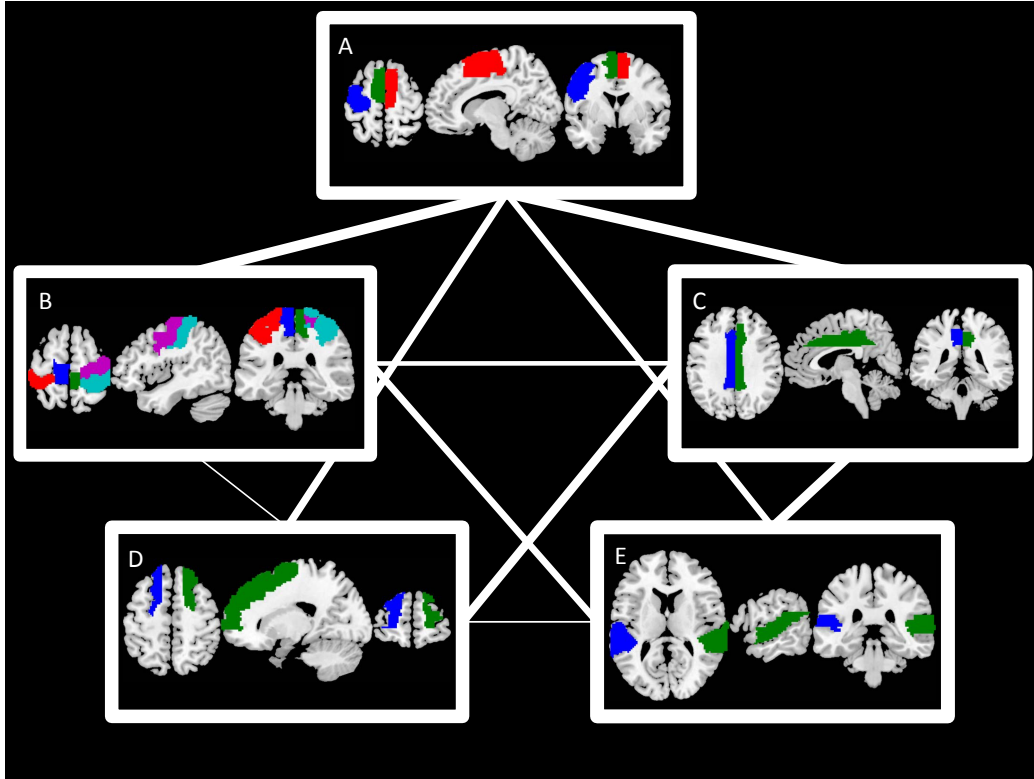


Figure 4: This figure shows a single cluster A composed of left and right supplementary motor area and left precentral gyrus. Also, the 4 clusters with highest between cluster link probability to this cluster are shown. These 4 clusters are (B, $\rho_{A,B} = 0.732$) left and right postcentral gyrus, left and right paracentral lobule and right precentral gyrus; (C, $\rho_{A,C} = 0.714$) left and right middle cingulate gyrus; (D, $\rho_{A,D} = 0.516$) left and right superior frontal gyrus; (E, $\rho_{A,E} = 0.456$) left and right superior temporal gyrus. The line widths between clusters reflect the link probabilities between clusters, likewise the widths of the boxes reflect the within-cluster link probabilities.

546 Figure 5 shows the clustering similarity both within the same link density
 547 and between different link densities for IRM, BCD, and IDM, respectively.
 548 IRM and BCD showed a similar pattern with increasing clustering similarity
 549 with increasing link density. When considering the link densities 8%, 16%,

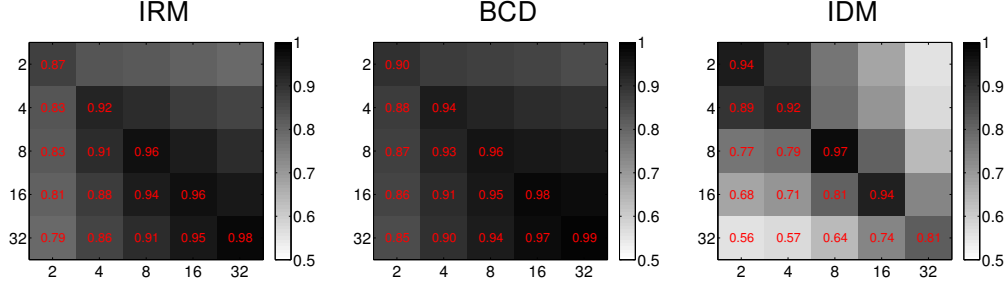


Figure 5: Mean NMI between clusterings found with different graph link densities for IRM, BCD, and IDM, respectively.

and 32% the mean NMI between the clusterings were all above 0.91, reflecting high similarity. Comparing the similarity between low and high link densities reveal lower similarity, for instance the mean NMI between 2% and 32% were 0.79 and 0.85 for IRM and BCD, respectively. BCD showed in general higher NMI values than IRM. For IDM the pattern was opposite, with decreasing similarity with increasing link density. Comparing clusterings between 2% and 32% for IDM revealed a relatively low NMI value of 0.56. The NMI values were in general lower for IDM than for IRM and BCD.

Figure 6 shows the solutions with the highest values of the posterior using BCD for different link densities. The tendency across different link densities is that clusters are very left-right symmetric.

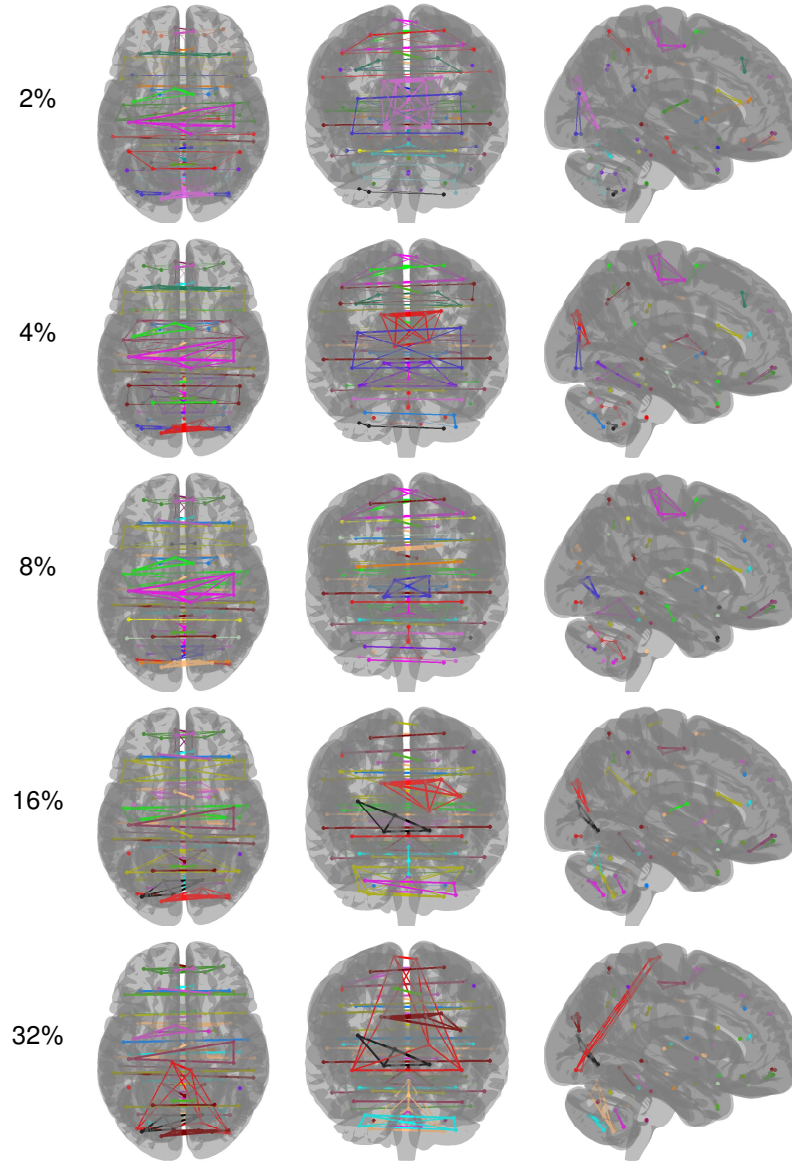


Figure 6: Clusterings found using BCD for different graph link densities.

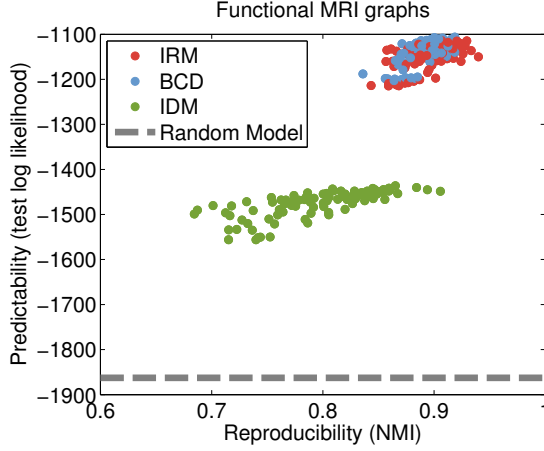


Figure 7: Reproducibility vs predictability plot for the three models using a link density of 8%. IDM and BCD showed better NMI and test log likelihood compared with IRM ($p < 0.0001$). BCD showed better predictability ($p = 0.023$) compared with IRM while IRM and BCD did not differ in reproducibility ($p = 0.15$).

3.2. Predictability and reproducibility

Figure 7 shows the PR scatter plot of the predictability versus reproducibility of the 3 methods using the NPAIRS split-half framework. Clearly, IRM and BCD performed better compared with IDM in both reproducibility and predictability as measured with NMI and test log likelihood ($p < 0.0001$, permutation test). IRM and BCD overlap, however, when testing for differences BCD showed slightly better predictability than IRM ($p = 0.023$) while the two methods did not differ in reproducibility ($p = 0.15$). On average IRM estimated 29.6 (std=0.83) clusters while BCD estimated 34.8 (0.88) and IDM estimated 17.7 (1.13). The number of clusters reported here was estimated on half-splits of the subject sample and are therefore different from the numbers reported in table 1 for models estimated on the whole sample.

573 3.3. Predictability and reproducibility for various link densities

574 Figure 8 shows the mean data and its standard error for the repro-
575 ducibility, predictability, number of clusters, and modularity index within
576 and between the three datasets when varying link density. This is shown for
577 IRM, BCD, and IDM, as well as Infomap, Louvain modularity, and hierar-
578 chical clustering. The columns represent the different datasets (Copenhagen,
579 Leipzig, Beijing, and between datasets respectively). Inspecting clustering
580 reproducibility the general tendency was that BCD and IRM increased with
581 increasing link densities while the other methods tended to decrease. For
582 link densities greater than 4% IRM and BCD were superior to the other
583 methods. BCD performed better or on par with IRM across all datasets and
584 for all link densities. For high link densities Infomap produced only a single
585 cluster causing both the nominator and denominator in the NMI calculation
586 to be zero, thus these values are not shown.

587 BCD and IRM generally showed higher predictability compared with the
588 other methods for all datasets and link densities. For the three within dataset
589 analyses BCD performed better compared with IRM for low link densities,
590 for higher link densities these two methods were on par. Interestingly, hier-
591 archical clustering generally showed higher predictability and reproducibility
592 than IDM, Louvain, and Infomap. Please note that the test log likelihood
593 ratio cannot be compared directly between different link densities.

594 When inspecting the number of clusters estimated by the methods two
595 patterns are observed. For IRM and BCD the number of clusters increased
596 with increasing link density. The opposite is seen with the other methods
597 where the number of clusters decreased with increasing link density.

598 Not surprisingly, the Louvain method had higher modularity values for all
599 sets and link densities compared with the other methods. IRM and BCD had
600 comparable modularity but was generally lower than the other methods. IDM
601 had higher modularity compared with the two other probabilistic methods
602 IRM and BCD.

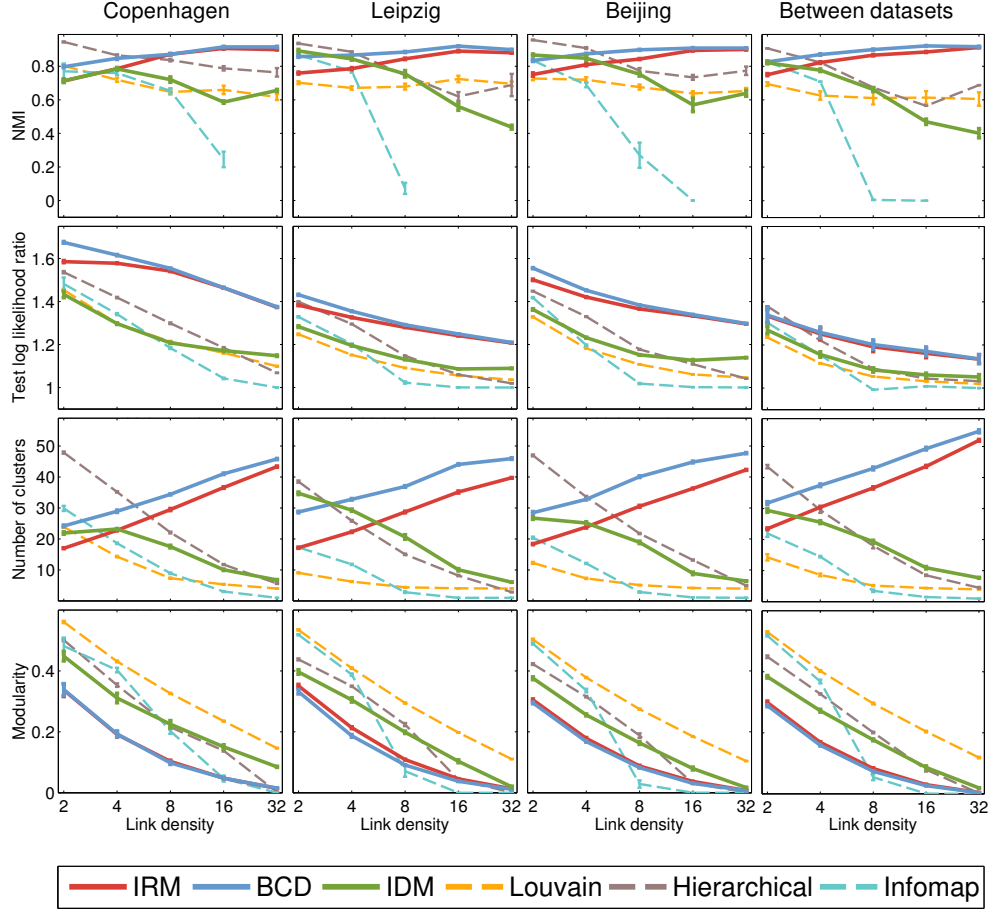


Figure 8: First row reproducibility (NMI), second row predictability (test log likelihood ratio), third row number of clusters, and fourth row modularity index as function of graph densities. Columns represent Copenhagen, Leipzig, Beijing, and between datasets respectively.

603 4. Discussion and conclusion

604 Our aim was to explore statistical models for finding structure in networks
605 at the intermediate level. Accumulated evidence points to the importance of

community structure in brain networks, hence, we tested three statistical link models, which differed in terms of the different restrictions that were imposed on how nodes are clustered. The IRM is a very flexible representation for graph clustering, in which nodes can be grouped together without having a high link density among them. The BCD is a constrained version of the IRM that discards such group structures by insisting on higher within-cluster interaction, conforming with the notion of community structure. Finally, the IDM model is further constrained to ignore potential differences in the way nodes in a community interact with other communities, inspired by the methods aimed at identifying structure based on the global modularity concept. These probabilistic models were compared against three other non-probabilistic methods for finding community structure in networks; Infomap, Louvain, and hierarchical clustering.

The results show a remarkable difference between the two models (IRM and BCD), which models the between-cluster linking, and the other methods, which does not specifically take the between-cluster linking into account. IRM and BCD had generally higher reproducibility (except for low link densities) and predictability and showed an increasing number of estimated clusters with increasing link densities. On the contrary, these two models had lower modularity index as compared with the other methods. Modularity is often used for node clustering in brain networks, however, the results shown here indicate that a modularity optimized partition is neither the most reproducible nor the most predictable.

In general IRM and BCD clustered few nodes together corresponding to interhemispheric homologues areas. IRM and BCD model the between-

631 cluster link probabilities, which allows one to inspect how different clusters
 632 link to each other, an example of this is shown in figure 4. While a low
 633 number of nodes in a specific cluster might not reveal a lot of information
 634 in itself, important characteristics can be extracted and interpreted when
 635 considering the information available from the between-cluster link probabilities.
 636 In such a way, the between-cluster link probabilities can reveal how the
 637 different clusters are linked, indicating the communication pattern between
 638 clusters. In contrast to these two most expressive models, IDM does not
 639 model specific between-cluster link probabilities. This results in larger clusters
 640 with relatively high within-cluster link probabilities, which are formed
 641 since the model does not care about specific relations to other clusters. These
 642 clusters are generally coarser and less nuanced compared to IRM and BCD
 643 rendering cluster interpretation difficult. An example of this is the large
 644 turquoise cluster shown in figure 3, which is composed of nodes in frontal,
 645 occipital, parietal, and temporal lobes.

646 The clusterings produced by IRM and BCD were very similar with mean
 647 NMI between clusterings of 0.94 at 8% link density. The similarity between
 648 the representations of IRM and BCD indicates that the flexibility of IRM is
 649 not needed when modeling rs-fMRI data. Even though IRM is able to cluster
 650 nodes such that the clustering does not obey the community structure, we see
 651 that IRM in general does produce clusterings which are very similar to BCD.
 652 The difference between BCD and IRM was most pronounced for smaller
 653 link densities suggesting that despite the large similarity between IRM and
 654 BCD it helps having the community structure constraint on the clustering.
 655 This is most evident for smaller link densities where the graphs contain less

656 information about the network. The better performance of BCD adds to
657 the evidence that coordinated activation in the resting state is community
658 structured.

659 By invoking a non-parametric Bayesian approach, the three modeling
660 schemes considered are less sensitive to conventional model specification is-
661 sues such as determining the number of communities as the number of clusters
662 is inferred during model inference. However, the models' hyper-parameters
663 still need to be set. In this study a uniform distribution was used as prior
664 for the link probabilities (obtained by setting $\beta = 1$) and the CRP hyper-
665 parameter α was set to 1, however other strategies could be considered. For
666 instance, given the Bayesian framework it would be straightforward to sam-
667 ple the hyper-parameters as part of the model inference (Kemp et al., 2006).
668 Our analysis scheme is a population level model, as we enforced graphs (sub-
669 jects) to share the model's link probability matrix. The choice of fixing the
670 link probabilities across subjects was done partly for evaluation purposes as
671 it allows us to estimate the test likelihood for unseen data and thus allows us
672 to estimate the models' predictability. However, the assumption that all sub-
673 jects have similar linking between clusters with no inter-subject variability
674 is somehow sub-optimal. Extending the models to allow for individual sub-
675 ject link probabilities is straight-forward (Mørup et al., 2010; Andersen et al.,
676 2012a). The results can be seen as compressed networks, where the new nodes
677 are formed by the clusters and (weighted) links are given by the individual
678 subject link probabilities. This enables test for group differences in link prob-
679 abilities or correlating with behavioral or personality measures where specific
680 between-cluster linking can be considered and enables a more specific conclu-

681 sion about how, e.g., different population groups differ in linking structure.
682 Using models which allow for individual subject link probabilities generally
683 result in fewer clusters than models which restrict link probabilities to be
684 equal across subjects (data not shown). This can be attributed to individual
685 subject link probabilities causing a more flexible model, thereby capturing
686 some of the flexibility which was previously accounted for by additional clus-
687 ters.

688 A number of studies have reported relevance of the conventional network
689 modularity measure to important cognitive measures, such as short term
690 memory capacity, reaction time etc. (Bassett et al., 2011; Stevens et al., 2012;
691 Meunier et al., 2009). Our findings suggest that there is important structure
692 in resting state networks beyond the global modularity. The rich link struc-
693 tures of the relational models can be seen as a way of inferring functional
694 integration at the inter-community level as discussed in (Hagmann et al.,
695 2008; Sporns, 2013). Hence, an interesting open question is how to convert
696 the flexible representations of the IRM and BCD to summary statistics that
697 can be used as bio-markers. Indeed, initial evidence for the relevance of the
698 community level link density (ρ) as a bio-marker for multiple sclerosis was
699 presented in Mørup et al. (2010)

700 When constructing the graphs one have to make decisions on how to de-
701 fine nodes and links. In this paper we used the brain regions from the AAL
702 atlas (Tzourio-Mazoyer et al., 2002) to define nodes, which enables compar-
703 ison with a large body of existing literature as the AAL atlas is the most
704 commonly used atlas in the fMRI brain network literature (Stanley et al.,
705 2013). The AAL regions have, however, been criticised for not reflecting

706 homogeneous functional units (Craddock et al., 2012). For instance, some
 707 of the AAL regions are rather large and thus could include more functional
 708 sub-units, which, when averaged together, degrade the functional connectiv-
 709 ity to other regions. Similarly, if a functional unit lies between two or more
 710 AAL regions they will be purely represented. The main purpose of this pa-
 711 per was to compare different models and not, per se, interpret the resulting
 712 clusterings. The AAL definition thus allow for a broad comparison of the
 713 results with other methods already reported using this atlas. However, using
 714 a higher resolution network, e.g. by invoking an initial parcellation of voxels
 715 into functionally coherent units (Craddock et al., 2012), it will be possible to
 716 make more interesting neurobiological interpretations of the resulting clusters
 717 and their interactions. Likewise, the measure used for forming links between
 718 nodes have a great impact on the network. Here we used Pearson correlation
 719 between nodes' time series. As described in the introduction, a high correla-
 720 tion between two nodes can be found simply if the two nodes are both highly
 721 correlated with a third node. The use of partial correlations or the inverse
 722 covariance matrix (Varoquaux and Craddock, 2013) can remove correlations
 723 mediated by a third node and thus remove this transiency effect. However,
 724 partial correlations are less stable and are therefore also less reproducible
 725 than simple correlations.

726 The models presented here use simple graphs, that is, unweighted and
 727 undirected graphs, which requires that the correlation matrices are thresh-
 728 olded at a certain level. The results show that the choice of threshold have
 729 an impact on the resulting clusters and that different methods is affected
 730 differently by increasing the threshold. However, for IRM and BCD the

consistency between the found clusterings higher thresholds (8%, 16%, 32%) were all very high as revealed by mean NMI all above 0.91. The exact choice of threshold is somewhat arbitrary to the problem as there is no natural threshold for which nodes can be said to be functionally connected. In addition, large negative correlations between nodes could provide important information to the network as well. However, negative coupling between nodes are by nature different from positive couplings, and thus should be considered differently in the network. Choosing a high threshold (meaning low link density) will fragment the network, that is, parts of the network or even single nodes will be unconnected to the rest of the network. In fact, in the networks presented here a number of nodes has very low or zero node degrees and are thus disconnected to the remaining network. An example of such nodes is seen in figure 3, where the IRM have clustered together a group of nodes¹ with low linking to the rest of the network (the cluster is best seen as the bright diagonal element in the lower right corner of the link probability matrix in the top panel of figure 3). These nodes are similar in the sense that they have low node degrees and can thus be represented as a 'null'-cluster. A similar 'null'-cluster² is found with the IDM model. For this cluster the within-cluster link probability is actually lower than the shared

¹Green cluster composed of Amygdala L+R, Temporal Pole Mid L+R, Olfactory L+R, Pallidum L+R, Vermis 1 2, Vermis 3, Vermis 10, Cerebellum 3 L+R, Cerebellum 10 L+R. See Figure Appendix C.

²Red cluster composed of Amygdala L+R, Cerebellum 3 L, Cerebellum 7b R, Cerebellum 10 L+R, Olfactory L+R, Pallidum L+R, Temporal Pole Mid L+R, Vermis 1 2, Vermis 3, Vermis 7, Vermis 9, Vermis 10.

750 between-cluster link probability. For the BCD model this null-cluster is split
 751 into several smaller clusters which have slightly higher within-cluster link
 752 probabilities than between-cluster link probabilities to other clusters, thus
 753 conforming to the definition of the community model. Given the somewhat
 754 arbitrary thresholding for binary graphs, an interesting future direction is
 755 to model dense weighted graphs. In fact, a modification of the IRM have
 756 already been proposed, which models dense weighted graphs. The normal
 757 Infinite Relational Model (nIRM) (Herlau et al., 2012) models weighted links
 758 with a normal distribution instead of the Bernoulli distribution for binary
 759 links. This means that the correlation between nodes are modelled directly
 760 without thresholding. The relational models have also been extended to
 761 model hierarchical grouping structure and to allow for nodes to be members
 762 of multiple clusters, please see (Schmidt and Mørup, 2013) for an overview.

763 In conclusion, we evaluated three different Bayesian models for finding
 764 structure in rs-fMRI graphs and compared them with 3 other methods for
 765 node clustering in complex networks. We showed that BCD performs best
 766 compared to IRM and IDM in terms of predictability and reproducibility.
 767 This suggests that (1) rs-fMRI data adhere to the community structure and
 768 (2) modeling specific between-cluster linking improves predictability and re-
 769 producibility.

770 *Toolbox*

771 A Matlab toolbox for performing the experiments conducted in this paper
 772 can be found at <https://brainconnectivity.compute.dtu.dk/>

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777 **5. References**

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942 **Appendix A. FCON1000 data**

943 Data included from Beijing Zang (data included in Beijing_Zang_part2.tar):
944 sub20127, sub20246, sub20765, sub20948, sub21115, sub22201, sub22595,
945 sub22661, sub22715, sub22890, sub26713, sub28206, sub28403, sub28698,
946 sub28792, sub28801, sub28907, sub28965, sub29590, sub29785, sub30272,
947 sub30310, sub30556, sub30616, sub30988, sub31058, sub31729, sub32517,
948 sub32587, sub33747, sub33943, sub33991, sub34895, sub34943, sub35309,
949 sub35776, sub35806, sub36580, sub36942, sub37602, sub38602, sub39725.

950 Data included from Leipzig:
951 sub00321, sub01002, sub02075, sub07097, sub07374, sub07516, sub07786,
952 sub18698, sub23427, sub25344, sub31577, sub31637, sub36858, sub37308,
953 sub41241, sub47452, sub49383, sub52507, sub52858, sub53063, sub53394,
954 sub59494, sub59709, sub59861, sub61373, sub63957, sub64446, sub72508,
955 sub75022, sub75886, sub77802, sub80206, sub80552, sub85213, sub90843,
956 sub92903, sub94784.

957 Appendix B. Inference

958 Appendix B.1. IRM

959 As stated in section 2.4 the generative model for the Infinite Relational
960 Model is

| Infinite Relational Model | |
|---------------------------|--|
| Cluster assignments: | $\mathbf{z} \sim \text{CRP}(\alpha)$ |
| Link probabilities: | $\rho_{k,l} \sim \text{Beta}(\beta, \beta)$ |
| Links: | $A_{i,j}^{(n)} \sim \text{Bernoulli}(\rho_{z_i, z_j})$ |

961 For brevity we define the joint set of graphs as $\mathbf{A} = \{\mathbf{A}^{(1)}, \dots, \mathbf{A}^{(N)}\}$. The
962 Bernoulli likelihood can then be written as:

$$\begin{aligned}
963 \quad P(\mathbf{A}|\mathbf{z}, \boldsymbol{\rho}) &= \prod_n \prod_{j>i} \rho_{z_i, z_j}^{A_{i,j}^{(n)}} (1 - \rho_{z_i, z_j})^{(1-A_{i,j}^{(n)})} \\
964 &= \prod_{j>i} \rho_{z_i, z_j}^{(\sum_n A_{i,j}^{(n)})} (1 - \rho_{z_i, z_j})^{(N - \sum_n A_{i,j}^{(n)})} \\
965 &= \prod_{k \geq l} \rho_{k,l}^{N_{k,l}^+} (1 - \rho_{k,l})^{N_{k,l}^-},
\end{aligned}$$

966 where $N_{k,l}^+$ and $N_{k,l}^-$ is the total number of links and nonlinks for all graphs
967 between cluster k and l , respectively and N is the number of graphs (sub-
968 jects). The prior for the link probabilities is a symmetric Beta distribution
969 and can be written as

$$970 \quad P(\boldsymbol{\rho}|\beta) = \prod_{k \geq l} \frac{\Gamma(2\beta)}{\Gamma(\beta)^2} \rho_{k,l}^{\beta-1} (1 - \rho_{k,l})^{\beta-1}$$

971 where $\Gamma(x) = (x-1)!$ is the gamma function. The CRP prior for the node
 972 partition can be written as

$$973 \quad P(\mathbf{z}|\alpha) = \frac{\alpha^K \Gamma(\alpha) \prod_k \Gamma(n_k)}{\Gamma(J + \alpha)}, \quad (\text{B.1})$$

974 where J is the number of nodes per graph, n_k is the number of nodes as-
 975 signed to cluster k and K is the number of clusters. These distributions are
 976 combined to yield the joint distribution for the IRM:

$$\begin{aligned} 977 \quad P(\mathbf{A}, \mathbf{z}, \boldsymbol{\rho}|\alpha, \beta) &= P(\mathbf{A}|\mathbf{z}, \boldsymbol{\rho}) P(\boldsymbol{\rho}|\beta) P(\mathbf{z}|\alpha) \\ 978 &= \left[\prod_{k \geq l} \rho_{k,l}^{N_{k,l}^+} (1 - \rho_{k,l})^{N_{k,l}^-} \right] \left[\prod_{k \geq l} \frac{\Gamma(2\beta)}{\Gamma(\beta)^2} \rho_{k,l}^{\beta-1} (1 - \rho_{k,l})^{\beta-1} \right] \\ 979 &\quad \times \left[\frac{\alpha^K \Gamma(\alpha) \prod_k \Gamma(n_k)}{\Gamma(J + \alpha)} \right] \\ 980 &= \left[\prod_{k \geq l} \frac{\Gamma(2\beta)}{\Gamma(\beta)^2} \rho_{k,l}^{N_{k,l}^+ + \beta - 1} (1 - \rho_{k,l})^{N_{k,l}^- + \beta - 1} \right] \\ 981 &\quad \times \left[\frac{\alpha^K \Gamma(\alpha) \prod_k \Gamma(n_k)}{\Gamma(J + \alpha)} \right] \end{aligned}$$

982 Now we can marginalize $\boldsymbol{\rho}$:

$$\begin{aligned} 983 \quad P(\mathbf{A}, \mathbf{z}, |\alpha, \beta) &= \int P(\mathbf{A}, \mathbf{z}, \boldsymbol{\rho}|\alpha, \beta) d\boldsymbol{\rho} \\ 984 &= \left[\prod_{k \geq l} \frac{B(N_{k,l}^+ + \beta, N_{k,l}^- + \beta)}{B(\beta, \beta)} \right] \left[\frac{\alpha^K \Gamma(\alpha) \prod_k \Gamma(n_k)}{\Gamma(J + \alpha)} \right] \end{aligned}$$

985 where $B(x, y) = \frac{\Gamma(x)\Gamma(y)}{\Gamma(x+y)}$ is the Beta function. Finally using Bayes' theorem
 986 we can find the posterior distribution of the assignment of a single node z_i

$$987 \quad P(z_i = l | \mathbf{A}, \mathbf{z}_{\setminus i}, \beta, \alpha) = \frac{P(\mathbf{A}, \mathbf{z}_{\setminus i}, z_i = l | \alpha, \beta)}{\sum_{l'} P(\mathbf{A}, \mathbf{z}_{\setminus i}, z_i = l' | \alpha, \beta)}$$

988 where $\mathbf{z}_{\setminus i}$ is the assignments of all nodes except node i . By writing out this
 989 equation and finding parts which change when a node is assigned to a cluster

990 (Schmidt and Mørup, 2013) we have that:

$$991 \quad P(z_i = l | \mathbf{A}, \mathbf{z}_{\setminus i}, \beta, \alpha) \propto \begin{cases} n_{l \setminus i} \prod_k \frac{B(N_{k,l}^{+ \setminus i} + r_{i,k}^+ + \beta, N_{k,l}^{- \setminus i} + r_{i,k}^- + \beta)}{B(N_{k,l}^{+ \setminus i} + \beta, N_{k,l}^{- \setminus i} + \beta)} & \text{if } n_{l \setminus i} > 0 \\ \alpha \prod_k \frac{B(r_{i,k}^+ + \beta, r_{i,k}^- + \beta)}{B(\beta, \beta)} & \text{otherwise.} \end{cases} \quad (\text{B.2})$$

992 $N_{k,l}^{+ \setminus i}$ and $N_{k,l}^{- \setminus i}$ is the number of links and nonlinks between clusters k and l
 993 not counting links from node i . $n_{l \setminus i}$ is the number of nodes assigned to cluster
 994 l disregarding the assignment of node i . $r_{i,k}^+$ and $r_{i,k}^-$ is the number of links
 995 and nonlinks from node i to any node in cluster k . This posterior likelihood
 996 can be evaluated efficiently since we only need to compute \mathbf{N}^+ and \mathbf{N}^- and
 997 evaluate the Beta function for entries affected by the considered assignment
 998 change. The posterior likelihood is used in the Gibbs sampler to infer the
 999 node assignments.

1000 *Appendix B.2. IDM*

1001 The generative model for the Infinite Diagonal Model is given by:

| Infinite Diagonal Model | |
|-------------------------|---|
| Cluster assignments: | $\mathbf{z} \sim \text{CRP}(\alpha)$ |
| Link probabilities: | $\rho_{k,l} \sim \begin{cases} \rho_k = \text{Beta}(\beta, \beta) & \text{if } k = l \\ \rho_b = \text{Beta}(\beta, \beta) & \text{otherwise.} \end{cases}$ |
| Links: | $A_{i,j}^{(n)} \sim \text{Bernoulli}(\rho_{z_i, z_j})$ |

1002 The Bernoulli likelihood can accordingly be written as:

$$1003 \quad P(\mathbf{A} | \mathbf{z}, \boldsymbol{\rho}) = \rho_b^{N_b^+} (1 - \rho_b)^{N_b^-} \left[\prod_k \rho_k^{N_k^+} (1 - \rho_k)^{N_k^-} \right],$$

1004 where N_k^+ and N_k^- is the number of links and nonlinks within cluster k and
 1005 N_b^+ and N_b^- is the total number of links and nonlinks which fall between
 1006 clusters. The prior for the link probabilities can be written as

$$1007 \quad P(\boldsymbol{\rho}|\beta) = \frac{\Gamma(2\beta)}{\Gamma(\beta)^2} \rho_b^{\beta-1} (1 - \rho_b)^{\beta-1} \left[\prod_k \frac{\Gamma(2\beta)}{\Gamma(\beta)^2} \rho_k^{\beta-1} (1 - \rho_k)^{\beta-1} \right]$$

1008 The prior for the node partition is the same as the IRM model (equation
 1009 B.1). The joint distribution for the IDM can then be written as:

$$\begin{aligned} 1010 \quad P(\mathbf{A}, \mathbf{z}, \boldsymbol{\rho}|\alpha, \beta) &= P(\mathbf{A}|\mathbf{z}, \boldsymbol{\rho}) P(\boldsymbol{\rho}|\beta) P(\mathbf{z}|\alpha) \\ 1011 &= \left[\rho_b^{N_b^+} (1 - \rho_b)^{N_b^-} \right] \left[\prod_k \rho_k^{N_k^+} (1 - \rho_k)^{N_k^-} \right] \\ 1012 &\quad \times \left[\frac{\Gamma(2\beta)}{\Gamma(\beta)^2} \rho_b^{\beta-1} (1 - \rho_b)^{\beta-1} \right] \left[\prod_k \frac{\Gamma(2\beta)}{\Gamma(\beta)^2} \rho_k^{\beta-1} (1 - \rho_k)^{\beta-1} \right] \\ 1013 &\quad \times \left[\frac{\alpha^K \Gamma(\alpha) \prod_k \Gamma(n_k)}{\Gamma(J + \alpha)} \right] \\ 1014 &= \frac{\Gamma(2\beta)}{\Gamma(\beta)^2} \rho_b^{N_b^+ + \beta - 1} (1 - \rho_b)^{N_b^- + \beta - 1} \\ 1015 &\quad \times \left[\prod_k \frac{\Gamma(2\beta)}{\Gamma(\beta)^2} \rho_k^{N_k^+ + \beta - 1} (1 - \rho_k)^{N_k^- + \beta - 1} \right] \\ 1016 &\quad \times \left[\frac{\alpha^K \Gamma(\alpha) \prod_k \Gamma(n_k)}{\Gamma(J + \alpha)} \right] \end{aligned}$$

1017 Now marginalizing over $\boldsymbol{\rho}$:

$$\begin{aligned} 1018 \quad P(\mathbf{A}, \mathbf{z}|\alpha, \beta) &= \int P(\mathbf{A}, \mathbf{z}, \boldsymbol{\rho}|\alpha, \beta) d\boldsymbol{\rho} \\ 1019 &= \frac{B(N_b^+ + \beta, N_b^- + \beta)}{B(\beta, \beta)} \left[\prod_k \frac{B(N_k^+ + \beta, N_k^- + \beta)}{B(\beta, \beta)} \right] \\ 1020 &\quad \times \left[\frac{\alpha^K \Gamma(\alpha) \prod_k \Gamma(n_k)}{\Gamma(J + \alpha)} \right] \end{aligned}$$

1021 Finally using Bayes' theorem we can find the posterior distribution of the
 1022 assignment of a single node z_i

$$1023 \quad P(z_i = l | \mathbf{A}, \mathbf{z}_{\setminus i}, \beta, \alpha) = \frac{P(\mathbf{A}, \mathbf{z}_{\setminus i}, z_i = l | \alpha, \beta)}{\sum_{l'} P(\mathbf{A}, \mathbf{z}_{\setminus i}, z_i = l' | \alpha, \beta)}$$

1024 By writing out this equation and finding parts which change when a node is
 1025 assigned to a cluster we find that:

$$1026 \quad P(z_i = l | \mathbf{A}, \mathbf{z}_{\setminus i}, \beta, \alpha) \propto$$

$$1027 \quad \begin{cases} n_{l \setminus i} \frac{B(N_l^{+ \setminus i} + r_{i,l}^+ + \beta, N_l^{- \setminus i} + r_{i,l}^- + \beta)}{B(N_l^{+ \setminus i} + \beta, N_l^{- \setminus i} + \beta)} \frac{B(N_b^{+ \setminus i} + \sum_{k \neq l} r_{i,k}^+ + \beta, N_b^{- \setminus i} + \sum_{k \neq l} r_{i,k}^- + \beta)}{B(N_b^{+ \setminus i} + \beta, N_b^{- \setminus i} + \beta)} & \text{if } n_{l \setminus i} > 0 \\ \alpha \frac{B(N_b^{+ \setminus i} + \sum_{k \neq l} r_{i,k}^+ + \beta, N_b^{- \setminus i} + \sum_{k \neq l} r_{i,k}^- + \beta)}{B(N_b^{+ \setminus i} + \beta, N_b^{- \setminus i} + \beta)} & \text{otherwise.} \end{cases} \quad (\text{B.3})$$

1028 $r_{i,l}^+$ and $r_{i,l}^-$ is the number of links and nonlinks from node i to any node in
 1029 cluster l .

1030 *Appendix B.3. BCD*

1031 This section will give a short description of the inference in the Bayesian
 1032 Community Detection (BCD) model, for further details please refer to Mørup
 1033 and Schmidt (2012). The generative model for BCD is given by:

Bayesian Community Detection

Cluster assignments : $\mathbf{z} \sim \text{CRP}(\alpha)$

Cluster gap : $\gamma \sim \text{Beta}(v, v)$

Link probability : $\rho_{k,l} \sim \begin{cases} \text{Beta}(\beta, \beta) & \text{if } k = l \\ \text{BetaInc}(\beta, \beta, w_{k,l}) & \text{otherwise.} \end{cases}$

where $w_{k,l} = \min[\gamma\rho_{ll}, \gamma\rho_{kk}]$

Links : $A_{i,j}^{(n)} \sim \text{Bernoulli}(\rho_{z_i, z_j})$

1034 If we let $\dot{\rho} = \{\rho_{k,l} | k = l\}$ and $\ddot{\rho} = \{\rho_{k,l} | k \neq l\}$ be the set of within and
 1035 between link probabilities respectively. Then the joint distribution can be
 1036 written as

$$\begin{aligned}
 1037 \quad P(\mathbf{A}, \mathbf{z}, \boldsymbol{\rho}, \gamma | \alpha, \beta) &= P(\mathbf{A} | \mathbf{z}, \boldsymbol{\rho}) P(\ddot{\rho} | \dot{\rho}, \gamma, \beta) P(\dot{\rho} | \beta) P(\gamma | v) P(\mathbf{z} | \alpha) \\
 1038 &= \left[\prod_{n=1}^N \prod_{j>i} \rho_{z_i, z_j}^{A_{i,j}^{(n)}} (1 - \rho_{z_i, z_j})^{1 - A_{i,j}^{(n)}} \right] \\
 1039 &\quad \times \left[\prod_{k>l} \frac{\rho_{k,l}^{\beta-1} (1 - \rho_{k,l})^{\beta-1}}{\text{B}_{x_{k,l}}(\beta, \beta)} \right] \left[\prod_{l=1}^K \frac{\rho_{l,l}^{\beta-1} (1 - \rho_{l,l})^{\beta-1}}{\text{B}(\beta, \beta)} \right] \\
 1040 &\quad \times \left[\frac{\gamma^{v-1} (1 - \gamma)^{v-1}}{\text{B}(v, v)} \right] \left[\frac{\alpha^K \Gamma(\alpha) \prod_k \Gamma(n_k)}{\Gamma(J + \alpha)} \right]
 \end{aligned}$$

1041

1042 Integrating over $\dot{\boldsymbol{\rho}}$:

$$\begin{aligned}
1043 \quad P(\mathbf{A}, \mathbf{z}, \dot{\boldsymbol{\rho}}, \gamma | \alpha, \beta) &= \int P(\mathbf{A}, \mathbf{z}, \boldsymbol{\rho}, \gamma | \alpha, \beta) d\dot{\boldsymbol{\rho}} \\
1044 &= \left[\prod_{k=1}^K \frac{\rho_{k,k}^{N_{k,k}^+ + \beta - 1} (1 - \rho_{k,k})^{N_{k,k}^- + \beta - 1}}{B(\beta, \beta)} \right] \\
1045 &\quad \times \left[\prod_{k>l} \frac{B_{x_{k,l}}(N_{k,l}^+ + \beta, N_{k,l}^- + \beta)}{B_{x_{k,l}}(\beta, \beta)} \right] \\
1046 &\quad \times \left[\frac{\gamma^{v-1} (1 - \gamma)^{v-1}}{B(v, v)} \right] \left[\frac{\alpha^K \Gamma(\alpha) \prod_k \Gamma(n_k)}{\Gamma(J + \alpha)} \right]
\end{aligned}$$

1047 Again, using Bayes theorem and eliminating terms which does not depend
 1048 on $\rho_{l,l}$ the marginal posterior reduces to

$$1049 \quad P(\rho_{l,l} | \mathbf{A}, \mathbf{z}, \dot{\boldsymbol{\rho}} \setminus \rho_{l,l}, \beta, \alpha, \gamma) \propto \rho_{l,l}^{N_{l,l}^+ + \beta - 1} (1 - \rho_{l,l})^{N_{l,l}^- + \beta - 1} \prod_{k \neq l} \frac{B_{x_{l,k}}(N_{k,l}^+ + \beta, N_{k,l}^- + \beta)}{B_{x_{k,l}}(\beta, \beta)}$$

1050 The conditional distribution for a node assignment is given as (Mørup and
 1051 Schmidt, 2012):

$$\begin{aligned}
1052 \quad P(z_i = l | \mathbf{A}, \mathbf{z}_{\setminus i}, \dot{\boldsymbol{\rho}}, \beta, \alpha, \gamma) &\propto \rho_{l,l}^{r_{i,l}^+} (1 - \rho_{l,l})^{r_{i,l}^-} \alpha^K n_{l \setminus i} \\
1053 &\quad \prod_{k \neq l} \frac{B_{x_{k,l}}(N_{k,l}^+ + r_{i,k}^+ + \beta, N_{k,l}^- + r_{i,k}^- + \beta)}{B_{x_{k,l}}(N_{k,l}^+ + \beta, N_{k,l}^- + \beta)}
\end{aligned}$$

1054 When terms which does not depend on γ are ignored the posterior reduces
 1055 to

$$1056 \quad P(\gamma | \mathbf{A}, \mathbf{z}, \dot{\boldsymbol{\rho}}, \beta, \alpha) \propto \gamma^{v-1} (1 - \gamma)^{v-1} \prod_{k>l} \frac{B_{x_{k,l}}(N_{k,l}^+ + \beta, N_{k,l}^- + \beta)}{B_{x_{k,l}}(\beta, \beta)}$$

1057 Appendix C. Clusters labels

| IRM | BCD | IDM | IRM | BCD | IDM |
|----------------------|----------------------|----------------------|---------------------|---------------------|---------------------|
| Frontal Mid Orb L | Frontal Mid Orb L | Frontal Mid Orb L | Insula L | Insula L | Insula L |
| Frontal Mid Orb R | Frontal Mid Orb R | Frontal Mid Orb R | Insula R | Insula R | Insula R |
| Frontal Sup Orb L | Frontal Sup Orb L | Frontal Sup Orb L | Rolandic Oper L | Rolandic Oper L | Rolandic Oper L |
| Frontal Sup Orb R | Frontal Sup Orb R | Frontal Sup Orb R | Rolandic Oper R | Rolandic Oper R | Rolandic Oper R |
| Hippocampus L | Hippocampus L | Hippocampus L | Heschl L | Heschl L | Heschl L |
| Hippocampus R | Hippocampus R | Hippocampus R | Heschl R | Heschl R | Heschl R |
| ParaHippocampal L | ParaHippocampal L | ParaHippocampal L | SupraMarginal L | SupraMarginal L | SupraMarginal L |
| ParaHippocampal R | ParaHippocampal R | ParaHippocampal R | SupraMarginal R | SupraMarginal R | SupraMarginal R |
| Thalamus L | Thalamus L | Thalamus L | Caudate L | Caudate L | Caudate L |
| Thalamus R | Thalamus R | Thalamus R | Caudate R | Caudate R | Caudate R |
| Parietal Inf L | Parietal Inf L | Parietal Inf L | Putamen L | Putamen L | Putamen L |
| Parietal Inf R | Parietal Inf R | Parietal Inf R | Putamen R | Putamen R | Putamen R |
| Temporal Pole Sup L | Temporal Pole Sup L | Temporal Pole Sup L | Angular L | Angular L | Angular L |
| Temporal Pole Sup R | Temporal Pole Sup R | Temporal Pole Sup R | Angular R | Angular R | Angular R |
| Calcarine L | Calcarine L | Calcarine L | Cingulum Post L | Cingulum Post L | Cingulum Post L |
| Calcarine R | Calcarine R | Calcarine R | Cingulum Post R | Cingulum Post R | Cingulum Post R |
| Lingual L | Lingual L | Lingual L | Frontal Med Orb L | Frontal Med Orb L | Frontal Med Orb L |
| Lingual R | Lingual R | Lingual R | Frontal Med Orb R | Frontal Med Orb R | Frontal Med Orb R |
| Cingulum Mid L | Cingulum Mid L | Cingulum Mid L | Rectus L | Rectus L | Rectus L |
| Cingulum Mid R | Cingulum Mid R | Cingulum Mid R | Rectus R | Rectus R | Rectus R |
| Cuneus L | Cuneus L | Cuneus L | Cerebellum 7b L | Cerebellum 7b L | Cerebellum 7b L |
| Cuneus R | Cuneus R | Cuneus R | Cerebellum 7b R | Cerebellum 7b R | Cerebellum 7b R |
| Occipital Sup L | Occipital Sup L | Occipital Sup L | Vermis 7 | Cerebellum 10 L | Cerebellum 10 L |
| Occipital Sup R | Occipital Sup R | Occipital Sup R | Vermis 9 | Cerebellum 10 R | Cerebellum 10 R |
| Occipital Inf L | Occipital Inf L | Occipital Inf L | Cerebellum 9 L | Cerebellum 3 L | Cerebellum 3 L |
| Occipital Inf R | Occipital Inf R | Occipital Inf R | Cerebellum 9 R | Cerebellum 3 R | Cerebellum 3 R |
| Occipital Mid L | Occipital Mid L | Occipital Mid L | Vermis 3 | Vermis 3 | Vermis 3 |
| Occipital Mid R | Occipital Mid R | Occipital Mid R | Amygdala L | Amygdala L | Amygdala L |
| Fusiform L | Fusiform L | Fusiform L | Amygdala R | Amygdala R | Amygdala R |
| Fusiform R | Fusiform R | Fusiform R | Temporal Pole Mid L | Temporal Pole Mid L | Temporal Pole Mid L |
| Paracentral Lobule L | Paracentral Lobule L | Paracentral Lobule L | Temporal Pole Mid R | Temporal Pole Mid R | Temporal Pole Mid R |
| Paracentral Lobule R | Paracentral Lobule R | Paracentral Lobule R | Olfactory L | Olfactory L | Olfactory L |
| Postcentral L | Postcentral L | Postcentral L | Olfactory R | Olfactory R | Olfactory R |
| Postcentral R | Postcentral R | Postcentral R | Pallidum L | Pallidum L | Pallidum L |
| Precentral R | Precentral R | Precentral R | Pallidum R | Pallidum R | Pallidum R |
| Precentral L | Precentral L | Precentral L | Vermis 10 | Vermis 10 | Vermis 10 |
| Supp Motor Area L | Supp Motor Area L | Supp Motor Area L | Vermis 12 | Cerebellum 9 L | Cerebellum 9 L |
| Supp Motor Area R | Supp Motor Area R | Supp Motor Area R | Cerebellum 3 R | Cerebellum 9 R | Cerebellum 9 R |
| Parietal Sup L | Parietal Sup L | Parietal Sup L | Cerebellum 10 L | Vermis 7 | Cerebellum 3 R |
| Parietal Sup R | Parietal Sup R | Parietal Sup R | Cerebellum 10 R | Vermis 8 | Cerebellum 3 R |
| Precuneus L | Precuneus L | Precuneus L | Cerebellum 3 L | Vermis 9 | Cerebellum 7b L |
| Precuneus R | Precuneus R | Precuneus R | Vermis 3 | Cerebellum 4 5 L | Cerebellum 4 5 L |
| Temporal Inf L | Temporal Inf L | Temporal Inf L | Cerebellum 4 5 L | Cerebellum 4 5 R | Cerebellum 4 5 R |
| Temporal Inf R | Temporal Inf R | Temporal Inf R | Vermis 4 5 | Vermis 4 5 | Vermis 4 5 |
| Temporal Sup L | Temporal Sup L | Temporal Sup L | Vermis 6 | Cerebellum 8 L | Cerebellum 8 L |
| Temporal Sup R | Temporal Sup R | Temporal Sup R | Cerebellum 8 L | Cerebellum 8 R | Cerebellum 8 R |
| Temporal Mid L | Temporal Mid L | Temporal Mid L | Cerebellum 6 L | Cerebellum 6 L | Cerebellum 6 L |
| Temporal Mid R | Temporal Mid R | Temporal Mid R | Cerebellum 6 R | Cerebellum 6 R | Cerebellum 6 R |
| Frontal Mid L | Frontal Mid L | Frontal Mid L | Cerebellum 8 R | Cerebellum 8 R | Cerebellum 8 R |
| Frontal Mid R | Frontal Mid R | Frontal Mid R | Cerebellum 6 L | Cerebellum 6 L | Cerebellum 6 L |
| Cingulum Ant L | Cingulum Ant L | Cingulum Ant L | Cerebellum 6 R | Cerebellum 6 R | Cerebellum 6 R |
| Cingulum Ant R | Cingulum Ant R | Cingulum Ant R | Cerebellum Crust1 L | Cerebellum Crust1 L | Cerebellum Crust1 L |
| Frontal Inf Oper L | Frontal Inf Oper L | Frontal Inf Oper L | Cerebellum Crust1 R | Cerebellum Crust1 R | Cerebellum Crust1 R |
| Frontal Inf Oper R | Frontal Inf Oper R | Frontal Inf Oper R | Cerebellum Crust2 L | Cerebellum Crust2 L | Cerebellum Crust2 L |
| Frontal Inf Tri L | Frontal Inf Tri L | Frontal Inf Tri L | Cerebellum Crust2 R | Cerebellum Crust2 R | Cerebellum Crust2 R |
| Frontal Inf Tri R | Frontal Inf Tri R | Frontal Inf Tri R | | | |
| Frontal Sup L | Frontal Sup L | Frontal Sup L | | | |
| Frontal Sup R | Frontal Sup R | Frontal Sup R | | | |
| Frontal Sup Medial L | Frontal Sup Medial L | Frontal Sup Medial L | | | |
| Frontal Sup Medial R | Frontal Sup Medial R | Frontal Sup Medial R | | | |
| Frontal Inf Orb L | Frontal Inf Orb L | Frontal Inf Orb L | | | |
| Frontal Inf Orb R | Frontal Inf Orb R | Frontal Inf Orb R | | | |

Figure C.9: Labels from the extracted clusters using IRM, BCD, and IDM. The colors correspond to the clusters from figure 3.